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# Long-term in vivo immune tracking nanoplatform based on Ag<sub>2</sub>S quantum dots for the photothermal immunotherapy of breast cancer

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## Abstract

**Background** Photothermal immunotherapy, as a promising technique in cancer treatment, offering precise eradication of tumor tissue, minimal adverse effects, and reduced risk of recurrence and metastasis. However, due to the instability of tracer function after photothermal immunotherapy, the long-term in vivo tracing is still a significant challenge, thereby greatly impeding the comprehensive assessment of immune response and drug delivery outcomes.

**Results** Here, we successfully demonstrated the feasibility of stable long-term in vivo immune tracking of photothermal immunodiagnosis and immunotherapy for breast cancer. The biocompatible and stable Ag<sub>2</sub>S quantum dots, with an average size of 3.8 nm, were coated with ovalbumin (OVA) and loaded with immune adjuvant imiquimod (R837). This synthesized Ag<sub>2</sub>S@OVA-R837 nanovaccine exhibited an excellent photothermal response upon near-infrared irradiation at 808 nm and effectively activated dendritic cells. In an in vivo breast tumor mouse model, we demonstrated that this nanoplatform, in combination with laser treatment, significantly improved long-term survival rates, reduced tumor size, and elicited robust immune responses.

**Conclusions** The results support that Ag<sub>2</sub>S@OVA-R837 is a promising photothermal immunotherapy (PIT) tracer nanoplatform to feedback immunoefficacy of therapeutics and holds great promise for precise treatment and diagnosis of malignant tumors, providing a novel avenue for visualizing the in vivo distribution and trafficking of functional therapeutics.

**Keywords** Ag<sub>2</sub>S quantum dots, Photothermal immunotherapy, Long-term tracking

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## Background

Cancer has emerged as one of the leading causes of mortality worldwide [1, 2], with a recent report indicating 19.3 million new cases diagnosed across 185 countries recently [2]. Therefore, cancer therapy remains a crucial research topic in biomedical research. Current treatment strategies primarily include surgery, radiotherapy, chemotherapy, and endocrine therapy, during which the balance between effectively killing tumor cells and minimizing damage to healthy tissue is critical. Additionally, the traditional therapies often struggle to completely eradicate tumor cells, leading to significant challenges with recurrence and metastasis.

In the rapidly advancing field of cancer therapeutics, photothermal nanomaterials exhibit significant potential by enabling targeted photothermal therapy (PTT) while also facilitating the delivery of anticancer agents or immunostimulants [3–13]. These advances represent a new frontier in combating various types of cancers such as melanoma, colon cancer, and human papillomavirus-associated malignancies [14]. Over the past few years, single-walled carbon nanotubes (SWNTs), black phosphorus nanoparticles [15–18], gold nanorods (GNRs) [19–21], and iron oxide nanoparticles [22] have been demonstrated as effective contrast agents for multimodal imaging techniques such as magnetic resonance imaging (MRI) [22] and computed tomography (CT) [23]. However, these nanomaterials often face limitations, such as reduced imaging capabilities or weakened signals after PTT process, posing significant difficulties for long-term in vivo tracking [24–30]. This issue is particularly critical when assessing drug delivery and efficacy outcomes, highlighting the need for novel photothermal materials to drive further advancements in PTT applications.

Among various candidate materials, quantum dots (QDs) have emerged as promising candidates for in vivo fluorescence probes due to their stable near-infrared (NIR)-I excitation and NIR-II fluorescence emission, which enable deep tissue penetration in clinical optical imaging [16, 31–33].  $\text{Ag}_2\text{S}$  QDs stand out because of their cost-effectiveness, high biocompatibility, and robust fluorescence stability. Ongoing studies on  $\text{Ag}_2\text{S}$  QDs are currently focused on their synthesis, fluorescence properties, and therapeutical functionalities, such as self-fluorescent  $\text{Ag}_2\text{S}$  materials [34], excitation and emission properties of  $\text{Ag}_2\text{S}$  QD [35], biocompatibility during photothermal therapy [36, 37], and chiral  $\text{Ag}_2\text{S}$  functional drugs [38] for therapeutic applications. Studies evaluating  $\text{Ag}_2\text{S}$  QDs' long-term in vivo immune tracking remain scarce. Since silver sulfide quantum dots offer a well balance between photothermal and fluorescent stability, making them effective in vivo tracers for a dynamic physical

feedback of immune evaluation after immunoactivation functionalization.

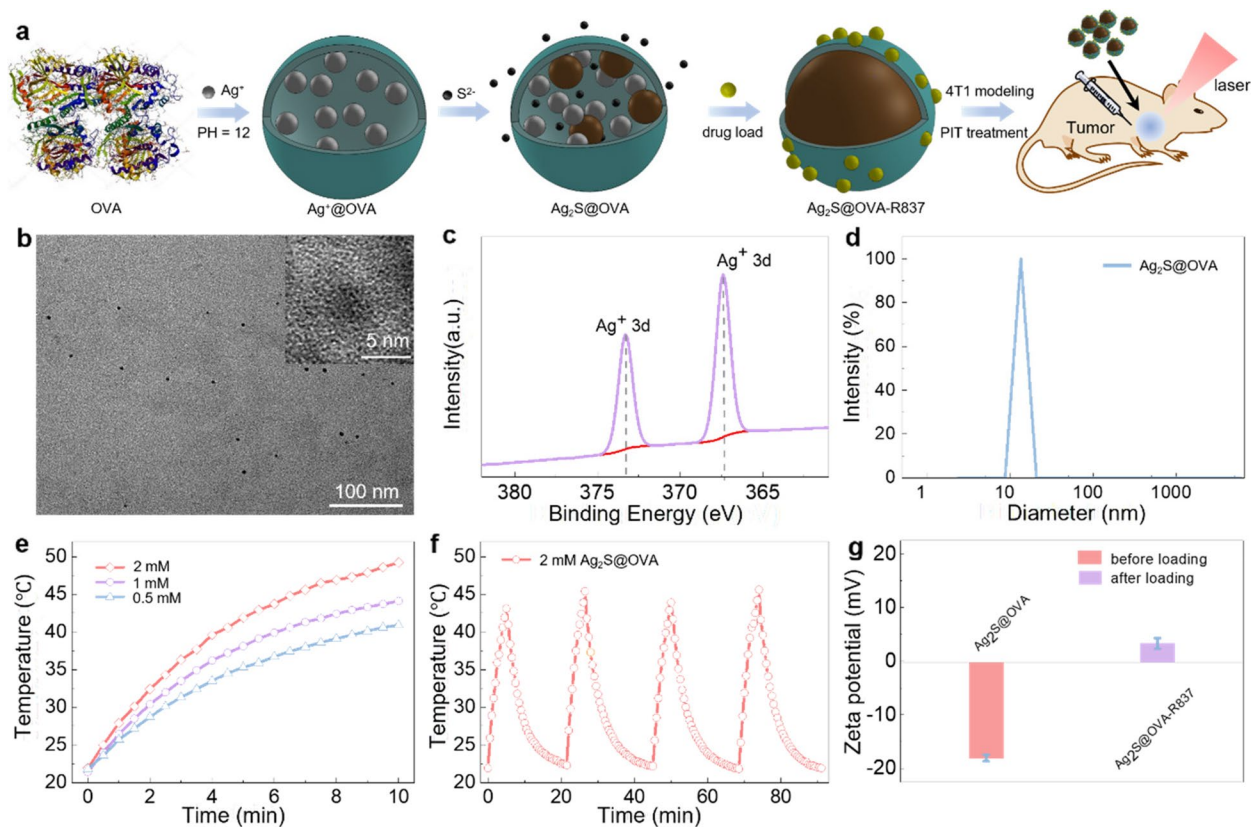
In this study, we developed  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  nanovaccines by combining  $\text{Ag}_2\text{S}$  QDs with ovalbumin (OVA) and imiquimod (R837) for the treatment of breast cancer using photothermal immunotherapy. In addition, the long-term monitoring of these nanovaccines' in vivo distribution was achieved using NIR-I excitation and NIR-II fluorescence imaging techniques, which enhanced their potential for further investigation and provided a visible means for auxiliary analysis. Our investigation involved synthesizing and characterizing the  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  nanovaccines, followed by evaluating their photothermal capabilities and immunostimulatory effects in vitro using mouse 4T1 breast cancer cells and DC2.4 dendritic cells, respectively. The efficacy of  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  in photothermal immunotherapy was evaluated in murine breast tumor model. At last, with the assistance of 808 nm laser excitation, the  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  nanovaccines served as in vivo tracers, enabling visualization and tracking of the animal's immune responses to photothermal immunotherapy. Our work highlighted a long-term in vivo immune-tracking nanoplatfrom and has great potentials for advancing the applications of cancer photothermal immunotherapy.

Existing photothermal immunotherapy technologies have shown promising results in tumor eradication, immune activation, and the prevention of recurrence and metastasis in animal and pre-clinical studies. However, verification of these approaches often relies on late-stage biochemical detection methods and long-term safety assessments. Our work aims to develop a long-term active traceable and photothermal material that remains capable of real-time dynamic monitoring after photothermal treatment. This approach provides a novel research perspective that could accelerated the clinical development cycle of new photothermal immune therapies and breast cancer treatments.

## Results

### Synthesis and characterization of $\text{Ag}_2\text{S}@ \text{OVA-R837}$

To enhance the immune activation effect, the  $\text{Ag}_2\text{S}$  QDs were synthesized and coated with the OVA antigen, a widely used antigen in immune research [39]. Afterwards, the FDA-approved immunomodulator R837, which targets Toll-like receptor 7, was loaded, creating a multimodal approach for breast cancer treatment (Fig. 1a). Transmission electron microscopy (TEM) images revealed that the  $\text{Ag}_2\text{S}$  cores possessed an average diameter of  $3.8 \pm 0.6$  nm (Fig. 1b). Complementary x-ray photoelectron spectroscopy (XPS) measurements corroborated the chemical identity of the  $\text{Ag}_2\text{S}$ , identifying the binding energy peaks at 373.3 and 367.4 eV for Ag



**Fig. 1** Synthesis and characterization of  $\text{Ag}_2\text{S}@ \text{OVA-R837}$ . **a** Schematic diagrams of the synthesis of  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  for the photothermal immunotherapy of 4T1 tumor model. **b** TEM images of the  $\text{Ag}_2\text{S}$  QDs. Inset: a zoom-in image of individual  $\text{Ag}_2\text{S}$  QDs. **c** XPS spectrum of  $\text{Ag}_2\text{S}@ \text{OVA}$  confirming the chemical content of Ag. **d** DLS analysis revealing the size distribution of  $\text{Ag}_2\text{S}@ \text{OVA}$  nanoparticles. **e** Photothermal response curves for  $\text{Ag}_2\text{S}$  QDs at different concentrations under 10 min of laser irradiation (808 nm,  $1.0 \text{ W/cm}^2$ ). **f** Repeated heating profiles for 2 mM  $\text{Ag}_2\text{S}@ \text{OVA}$  over four cycles of irradiation (808 nm,  $1.0 \text{ W/cm}^2$ ), demonstrating the photothermal stability. **g** Comparative zeta potential measurements of  $\text{Ag}_2\text{S}@ \text{OVA}$  and  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  nanoparticles

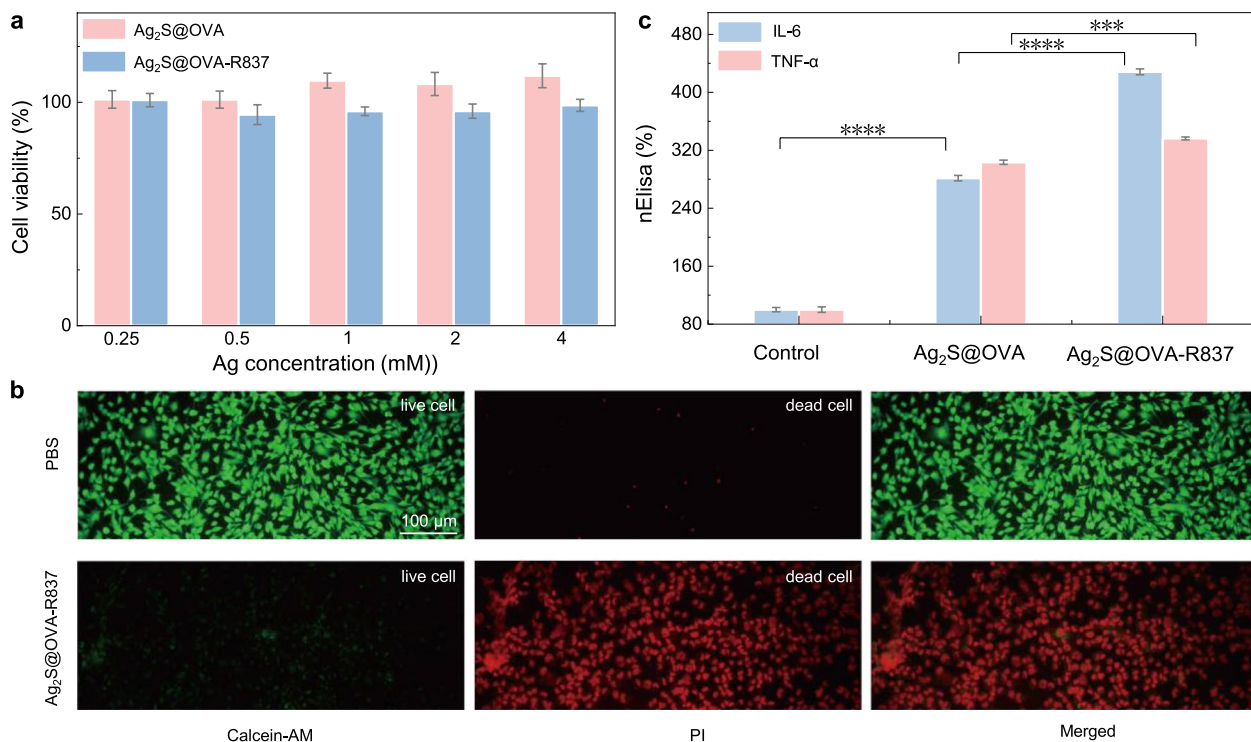
(Fig. 1c), and a peak at 162.8 eV for S (Additional file1: Fig. S1). Dynamic light scattering (DLS) analysis indicated that  $\text{Ag}_2\text{S}@ \text{OVA}$  nanoparticles had an approximate size of 13.5 nm with a narrow size distribution, suggesting excellent colloidal stability in phosphate-buffered saline (PBS) at a pH of 7.4 (Fig. 1d). The broadband absorption property of  $\text{Ag}_2\text{S}$  QDs was confirmed by the ultraviolet–visible absorption spectrum (Additional file1: Fig. S2).

To assess the photothermal properties,  $\text{Ag}_2\text{S}@ \text{OVA}$  solutions at varying concentrations (0.5, 1, and 2 mM Ag) were exposed to an 808 nm laser ( $1.0 \text{ W/cm}^2$ ) for 10 min. A concentration-dependent temperature increase can be clearly observed (Fig. 1e). The photothermal stability of  $\text{Ag}_2\text{S}@ \text{OVA}$  nanoparticles (2 mM Ag) was tested over four irradiation cycles (808 nm laser,  $1.0 \text{ W/cm}^2$ , 5 min of irradiation followed by a cooling period to room temperature). The nanoparticles showed consistent photothermal effects with no observable reduction in performance (Fig. 1f). Comparison across different concentrations

is provided in Additional file1: Fig. S3, which indicates that higher concentrations also maintain a stable temperature rise during the 5-min irradiation period. The electrostatic adsorption of R837 onto the  $\text{Ag}_2\text{S}@ \text{OVA}$  nanoparticles was evidenced by a shift in zeta potential from  $-18.04 \pm 0.61 \text{ mV}$  to  $3.31 \pm 0.98 \text{ mV}$ , confirming the successful formation of  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  (Fig. 1g). The loading efficiency of R837 onto  $\text{Ag}_2\text{S}@ \text{OVA}$  was quantified at 53.7%, using a standard calibration curve [7].

#### In vitro cytokine secretion detection

The cytotoxicity of  $\text{Ag}_2\text{S}$  QDs on 4T1 cells were assessed using the cell counting kit-8 (CCK-8) assay following a 24-h incubation period. The results demonstrated an absence of cytotoxicity, even at the highest concentration tested (4 mM of Ag, Fig. 2a). To further verify the safety of the materials, a hemolysis assay was conducted (Additional file1: Fig. S4). The hemolysis rates for both  $\text{Ag}_2\text{S}@ \text{OVA}$  and  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  were below 2%, measured at 1.45% and 0.27%, respectively. These results



**Fig. 2** In vitro cytokine secretion detection. **a** Cell viability of 4T1 cells after a 24-h incubation with different concentrations of nanoplateforms based on Ag<sub>2</sub>S QDs. **b** Fluorescence microscopy images showcasing 4T1 cells treated with 2 mM Ag<sub>2</sub>S@OVA-R837, followed by a 10-min irradiation with an 808 nm laser at a power density of 1.0 W/cm<sup>2</sup>. Live cells are stained with calcein AM (green fluorescence), while dead cells are stained with propidium iodide (PI, red fluorescence). **c** Normalized ELISA results indicating the secretion levels of IL-6 and TNF-α by DC2.4 cells in response to treatment with PBS, Ag<sub>2</sub>S@OVA, and Ag<sub>2</sub>S@OVA-R837. Data are represented as mean ± SD (*n* = 3). Statistical significance is denoted as ns (not significant), \*\*\**p* < 0.001, \*\*\*\**p* < 0.0001, based on two-way ANOVA

demonstrated that the Ag<sub>2</sub>S@OVA-R837 nanovaccines exhibited excellent biocompatibility.

The photothermal cytotoxic efficacy of the Ag<sub>2</sub>S@OVA-R837 nanovaccine was evaluated on 4T1 cells subjected to 10 min of laser irradiation (808 nm, 1.0 W/cm<sup>2</sup>). The assessment was conducted by fluorescent microscopy with live/dead staining, in comparison with a PBS control. Live cells were identified by calcein AM staining and emitted green fluorescence, while dead cells were marked by propidium iodide (PI) staining and emitted red fluorescence (Fig. 2b). The results demonstrate that Ag<sub>2</sub>S@OVA-R837 nanoparticles, upon laser irradiation, were effective in inducing cell death in 4T1 cells, providing preliminary in vitro evidence of its potential for tumor photothermal ablation. This supports the capability of the nanovaccines for subsequent in vivo studies. Further comparison of the in vivo photothermal effect is shown in Additional file1: Fig. S5.

Dendritic cells (DCs) are pivotal as antigen-presenting cells (APCs) in T cell activation. In our experiment, DC2.4 cells were incubated with PBS, Ag<sub>2</sub>S@OVA (2 mM Ag), and Ag<sub>2</sub>S@OVA-R837 (2 mM Ag) for 24 h. The secretion levels of the cytokines interleukin 6 (IL-6) and

tumor necrosis factor alpha (TNF-alpha) were measured using enzyme-linked immunosorbent assay (ELISA). Notably, a significant increase in both TNF-alpha and IL-6 secretion was detected following treatment with Ag<sub>2</sub>S@OVA, with a more pronounced elevation upon exposure to Ag<sub>2</sub>S@OVA-R837 (Fig. 2c).

These preliminary findings indicate that Ag<sub>2</sub>S@OVA-R837 can stimulate and enhance the immune response of APCs, thereby has a potential in activating naive T cells subsequently. This provides promising evidence for its capability to trigger immune responses in vivo, suggesting its potential as an immunotherapeutic agent.

#### In vivo antitumor efficacy

The in vivo antitumor efficacy of Ag<sub>2</sub>S@OVA-R837 (intratumoral administered at 2 mM Ag per 20 g mouse) combined with laser treatment (808 nm, 1.0 W/cm<sup>2</sup>, for 10 min) was evaluated in a murine model bearing 4T1 tumors. This treatment was compared against groups receiving Ag<sub>2</sub>S@OVA with laser treatment, PBS with laser treatment, and an untreated control group. Over an extended study period of more than 90 days, the survival rate of mice treated with Ag<sub>2</sub>S@OVA-R837 was the



highest at 83%, with complete tumor regression observed after 15 days (Fig. 3a–b). In contrast, mice receiving  $\text{Ag}_2\text{S}@ \text{OVA}$  and PBS with laser treatments showed survival rates of 33% and 17%, respectively, while the control group exhibited the most significant tumor growth and all animals succumbed within 33 days.

Serum levels of TNF- $\alpha$ , measured via ELISA, showed a marked increase after treatment with both  $\text{Ag}_2\text{S}@ \text{OVA}$  and notably  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  on days one, three, and seven (Fig. 3c). IL-6 levels peaked one day after the  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  treatment and then gradually declined. In mice treated with  $\text{Ag}_2\text{S}@ \text{OVA}$ , IL-6 levels rose more steadily, reaching the peak on day three before diminishing (Fig. 3d).

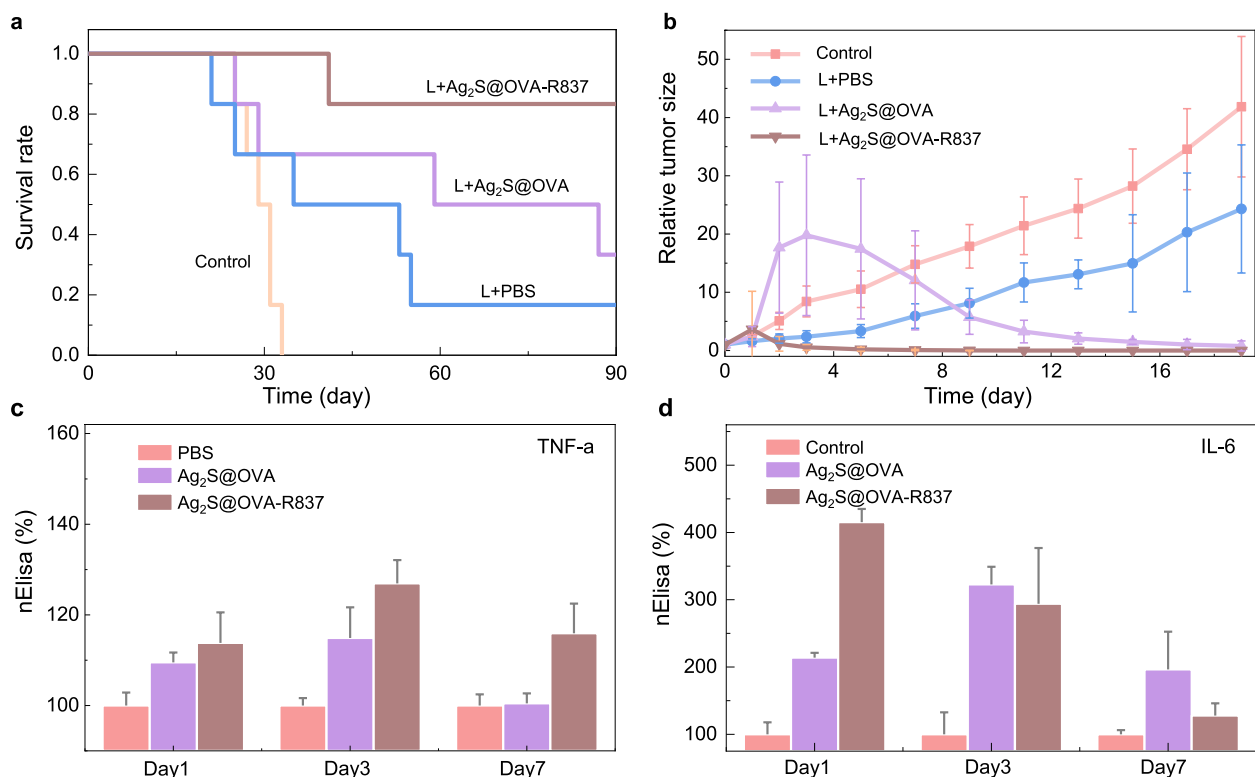
These findings collectively suggest that the  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  nanovaccines, when used in combination with PTT, effectively stimulate strong immune responses in vivo, highlighting its potential as a therapeutic strategy for cancer treatment.

#### Long-term in vivo immune tracking

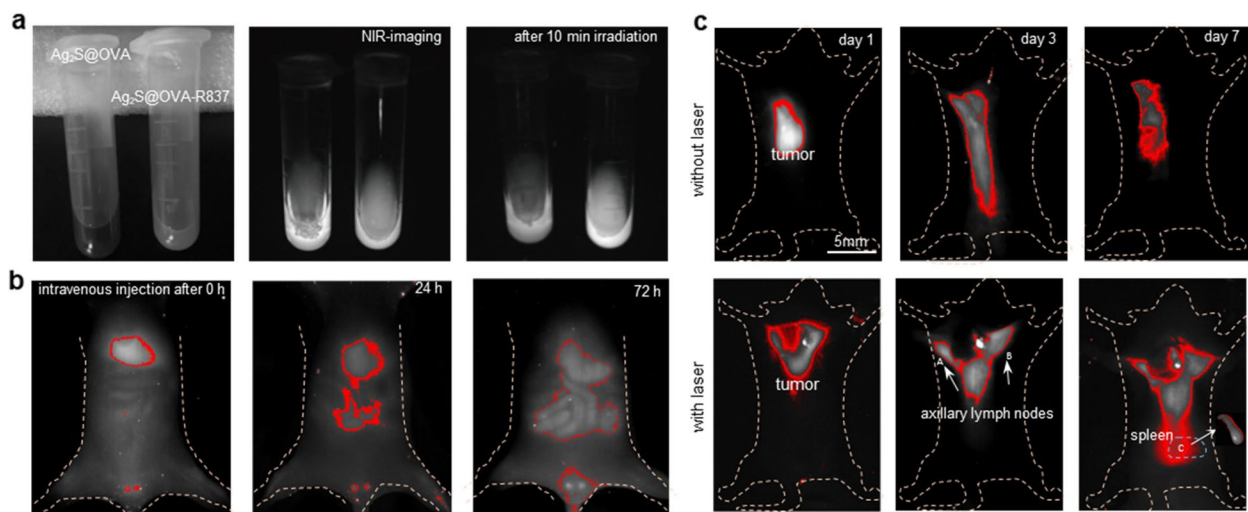
The development of stable and anti-photobleaching NIR-II fluorescence probes is crucial for advancing tracking

research. Despite their potential,  $\text{Ag}_2\text{S}$  QDs have not yet been explored as tracers for immune functionalization in vivo. The fluorescence emission spectrum of  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  upon excitation at 808 nm is shown in Additional file1:Fig. S6, featuring a distinct, narrow peak centered at 1096 nm, well within the desired NIR-II spectral region. Fluorescence imaging was conducted using an 1100 nm long-pass filter to capture the emission from suspensions of both  $\text{Ag}_2\text{S}@ \text{OVA}$  and  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  before and after 10 min of laser irradiation (808 nm, 1.0 W/cm<sup>2</sup>) in a dark setting. The absence of significant photobleaching suggests that these  $\text{Ag}_2\text{S}$  QDs remain stable after PTT (Fig. 4a).

To assess the potential for in vivo imaging,  $\text{Ag}_2\text{S}$  QDs were intravenously injected into healthy mice and tracked over a 3-day period. The images in Fig. 4b validate the successful in vivo visualization of the nanoparticles, with pronounced accumulation observed in the liver and intestines after 3 days. Furthermore,  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  was administered to tumor-bearing mice, with subsets of mice receiving PTT treatment (10 min, 808 nm, 1.0 W/cm<sup>2</sup>) and others not. In the absence of PTT, the  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  nanovaccines were initially detectable at the



**Fig. 3** In vivo antitumor efficacy. **a** Survival rates of the tumor-bearing mouse model post-treatment with PBS,  $\text{Ag}_2\text{S}@ \text{OVA}$ , or  $\text{Ag}_2\text{S}@ \text{OVA-R837}$ , each in combination with 10 min of laser irradiation (808 nm, 1.0 W/cm<sup>2</sup>). **b** Relative tumor volumes in BALB/c mice measured 15 days after treatment. **c** Serum TNF- $\alpha$  concentrations in mice at 1, 3, and 7 days post-treatment. **d** Serum IL-6 concentrations in mice at 1, 3, and 7 days post-treatment. The data for **a** and **b** are presented as mean  $\pm$  SD ( $n = 12$ ), while the results for **c** and **d** are depicted as mean  $\pm$  SD ( $n = 5$ )



**Fig. 4** Long-term in vivo immune tracking. **a** Near-infrared imaging of  $\text{Ag}_2\text{S}@ \text{OVA}$  and  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  pre- and post-laser irradiation. **b** NIR imaging over a period of 0–72 h in BALB/c mice post-tail vein injection with  $\text{Ag}_2\text{S}@ \text{OVA-R837}$  nanoparticles. **c–d** Near-infrared imaging from day 1 to day 7 in tumor-bearing BALB/c mice, without (**c**) and with (**d**) photothermal immunotherapy. A and B indicate axillary lymph nodes, while C denotes the spleen

tumor site on day 1, but the signal gradually dissipated and became undetectable over time (Fig. 4c). In contrast, PTT-treated mice not only exhibited nanoparticle localization within the tumor but also in both bilateral axillary lymph nodes, with marked visibility on day 3. By day 7 post-injection, the particles were also detectable within the spleen (Fig. 4d), indicating the possibility of inducing memory immune responses. This immune reaction was further demonstrated by the ex vivo analysis of excised axillary lymph nodes (Additional file1: Fig. S7).

## Discussion

Our work introduces a new real-time dynamic feedback method for the research and development of functional therapeutics for breast cancer, which could help shorten the clinical development cycle. However, practical applications are still limited by penetration depth, and the research is still primarily focused on animal models. Further studies are required to evaluate its long-term safety and in vivo metabolism in humans. Additionally, advancements in infrared imaging and endoscopy technology are needed to enhance the impact of this approach on the development of functional therapeutics for clinical breast cancer treatment.

## Conclusion

In conclusion, we have developed a versatile nanoplat-form utilizing  $\text{Ag}_2\text{S}$  QDs loaded with antigen and adjuvant for synergistic photothermal and immunotherapy. Owing to the unique optical properties of silver sulfide quantum dots, they effectively balance photothermal and

fluorescence stabilization functions. This makes them well-suited for long-term, real-time dynamic monitoring of in vivo biodistribution of photothermal immunofunctional therapeutics and other innovative agents. This system demonstrates remarkable in vivo tracking capabilities for over 7 days through NIR-II fluorescence imaging, even after continuous exposure to irradiation exceeding 10 min. Upon exposure to an 808 nm laser, the antitumor efficacy of our nanoplat-form was validated both in vitro and in vivo, highlighting its significant potential for diagnostic and therapeutic applications. This platform involves wrapping immune antigens and loading immune adjuvants to enhance immune responses after photothermal immunotherapy. The development of this nanoplat-form system holds promise for accurate treatment and post-treatment feedback of photothermal immunotherapy for malignant tumors, offering a new avenue for visualizing the in vivo distribution and trafficking of functional therapeutics.

## Methods

### Materials

Silver nitrate, sodium sulfide, sodium hydroxide, ovalbumin (OVA, molecular weight 44,287), Cell Counting Kit-8 (CCK-8), and imiquimod (R837) were purchased from Sigma-Aldrich. Fetal bovine serum (FBS), Roswell Park Memorial Institute (RPMI) 1640 medium, 0.25% trypsin–EDTA solution, as well as penicillin and streptomycin antibiotics were obtained from Gibco. Fluorescent dyes calcein AM and propidium iodide were supplied by Thermo Fisher Scientific.

### Cell culture and experiments

In this study, 4T1 cells were used as a breast cancer model. The cells were cultured in RPMI-1640 medium supplemented with 10% FBS and 1% penicillin–streptomycin and maintained at 37 °C in a humidified incubator with 5% CO<sub>2</sub>.

For the cytotoxicity assays, cells were incubated with Ag<sub>2</sub>S quantum dots (QDs) for 24 h at various silver (Ag) concentrations as specified in the text. Subsequently, the cells were rinsed to eliminate any unbound particles in the solution. Thereafter, 200 µL of cell medium containing 10% Cell Counting Kit-8 (CCK-8) solution was added to each well for a 2–3 h incubation period prior to absorbance measurement. Cell viability was then calculated using the following formula: Cell viability =  $(V_{\text{test}} - V_{\text{blank}}) / (V_{\text{PBS}} - V_{\text{blank}})$ , where “V” represents the absorbance values obtained from the microplate reader.

For cytotoxicity assays, 4T1 cells were incubated with Ag<sub>2</sub>S quantum dots (QDs) for 24 h at different silver (Ag) concentrations, as described in the text. After incubation, cells were washed to remove any unbound particles. Then, 200 µL of culture medium containing 10% CCK-8 solution was added to each well and incubated for 2–3 h before measuring absorbance. Cell viability was calculated using the following formula: Cell viability =  $(V_{\text{test}} - V_{\text{blank}}) / (V_{\text{PBS}} - V_{\text{blank}})$ , where “V” represents the absorbance values obtained from the microplate reader.

For fluorescence imaging, cells were treated with either PBS as a control or with Ag<sub>2</sub>S QDs at a concentration of 2 mM Ag, followed by irradiation with an 808 nm laser at a power density of 1.0 W/cm<sup>2</sup> for 10 min. After irradiation, the cells were washed and stained with calcein AM and propidium iodide (PI) for 30 min to facilitate imaging.

### Synthesis of Ag<sub>2</sub>S@OVA-R837

To synthesize Ag<sub>2</sub>S@OVA nanoparticles, silver nitrate (AgNO<sub>3</sub>, 20 mM) was added to an ovalbumin (OVA) solution (250 mg in 9 mL water) under continuous stirring. Sodium sulfide (Na<sub>2</sub>S, 0.1 M) was then added gradually to the mixture, which was stirred overnight at 55 °C to facilitate the formation of Ag<sub>2</sub>S@OVA nanoparticles. The resulting suspension was dialyzed for 24 h using a 100 kDa cut-off membrane in a buffer solution.

To load the immunostimulant imiquimod (R837) onto the nanoparticles, R837 (0.5 mg in 1 mL methanol) was added to the Ag<sub>2</sub>S@OVA solution. The mixture was stirred overnight in an open vial to allow evaporation of any residual methanol. The final product was dialyzed with a 10-kDa cut-off membrane to remove unbound R837 and subsequently freeze-dried. The loading

efficiency of R837 was quantified using UV absorption at 325 nm.

### Characterization and photothermal evaluation of Ag<sub>2</sub>S QDs

Transmission electron microscopy (TEM) was used to characterize Ag<sub>2</sub>S QDs using a JEM-2100 electron microscope (JEOL Ltd., Japan). X-ray photoelectron spectroscopy (XPS) analysis was performed with an AXIS SUPRA spectrometer (Shimadzu, Japan). The UV–Visible absorption spectrum was measured using a TU-1810 spectrophotometer (Puxitongyong, Beijing). Thermal measurements were conducted using an LE-LS-808 laser system (Feichuang, Shenzhen) with 808 nm laser irradiation, and temperature changes were detected using an infrared thermal detector. NIR-I (808 nm excitation) and NIR-II (emission at ~1100 nm) data were recorded using a Princeton Instrument (PI 2300).

### In vitro cytokine secretion analysis (DC2.4)

DC2.4 cells, an immature dendritic cell line, were used to assess cytokine secretion. Cells were treated with PBS, Ag<sub>2</sub>S@OVA nanoparticles, or Ag<sub>2</sub>S@OVA-R837 nanovaccines for 24 h. Secretion levels of tumor necrosis factor-α (TNF-α) and interleukin-6 (IL-6) were quantified using enzyme-linked immunosorbent assay (ELISA) to evaluate immune response.

### Animal model

Female BALB/c mice, aged 5–6 weeks, were obtained from Guangdong Medical Laboratory Animal Centre. A total of  $1 \times 10^5$  4T1 cells suspended in 0.1 mL PBS were subcutaneously injected into the primary mammary gland in the thoracic region. When the tumor volume reached 100–200 mm<sup>3</sup> (typically 7–10 days post-inoculation), the mice were randomly divided into four groups. Each group consisted of 12 mice for long-term survival analysis and 5 mice for serum cytokine measurement.

The treatment groups were as follows: (1) PBS (100 µL) with laser exposure (1.0 W/cm<sup>2</sup> for 10 min), (2) Ag<sub>2</sub>S@OVA-R837 ([Ag] = 10 mM, 100 µL) with laser exposure (1.0 W/cm<sup>2</sup> for 10 min), (3) Ag<sub>2</sub>S@OVA ([Ag] = 2 mM, 100 µL) with laser exposure (1.0 W/cm<sup>2</sup> for 10 min), and (4) Ag<sub>2</sub>S@OVA-R837 ([Ag] = 2 mM, 100 µL) without laser treatment.

Serum cytokine levels were measured in 5 mice from each group at 1, 3, and 7 days post-treatment using ELISA. During the experiments, anesthesia was administered using isoflurane, and euthanasia was performed by cervical dislocation.

### NIR-II in vivo tracking

NIR-II in vivo tracking was conducted using a non-invasive fluorescence imaging system equipped with an indium gallium arsenide (InGaAs) camera. Ag<sub>2</sub>S QDs were injected via the tail vein of healthy mice and monitored for 3 days to evaluate in vivo stability and metabolic pathways.

Furthermore, Ag<sub>2</sub>S@OVA-R837 was injected into a 4T1 tumor-bearing mouse model to investigate the in vivo biodistribution. The comparison was made between mice that received no laser treatment and those that underwent laser irradiation (1.0 W/cm<sup>2</sup> for 10 min) at 1, 3, and 7 days post-injection.

To assess biodistribution, Ag<sub>2</sub>S@OVA-R837 was injected into tumor-bearing mice, and comparisons were made between those with and without laser irradiation (1.0 W/cm<sup>2</sup> for 10 min) at 1, 3, and 7 days post-injection.

### Abbreviations

OVA	Ovalbumin
PTT	Photothermal therapy
SWNTs	Single-walled carbon nanotubes
GNRs	Gold nanorods
MRI	Magnetic resonance imaging
CT	Computed tomography
QDs	Quantum dots
NIR	Near-infrared
TEM	Transmission electron microscopy
XPS	X-ray photoelectron spectroscopy
DLS	Dynamic light scattering
PBS	Phosphate-buffered saline
CCK-8	Cell counting kit-8
PI	Propidium iodide
DCs	Dendritic cells
APCs	Antigen-presenting cells
IL-6	Interleukin 6
TNF-alpha	Tumor necrosis factor alpha
ELISA	Enzyme-linked immunosorbent assay
InGaAs	Indium gallium arsenide

### Supplementary Information

The online version contains supplementary material available at <https://doi.org/10.1186/s12915-025-02215-w>.

Additional file 1: Figures S1-S8. FigS1- The XPS spectrum revealing peak for S at approximately 162.2 eV. FigS2- UV-vis absorption spectrum of Ag<sub>2</sub>S@OVA. FigS3- Four thermal cycling profiles at different concentrations of Ag<sub>2</sub>S QDs. FigS4- Results of the hemolysis assay. FigS5- Monitoring the highest temperature of different groups. FigS6- Fluorescence emission spectrum upon excitation at 808 nm. FigS7- The ex vivo analysis of excised axillary lymph nodes. FigS8- The diagram illustrating the treatment process of Ag<sub>2</sub>S@OVA-R837 in vivo

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### Authors' contributions

JLW completed the entirety of the experimental work, encompassing material synthesis, cell culture, in vivo imaging experiments, and the preparation of the initial draft manuscript. ZLH and MW provided support for the immunological experiments. YBW and XFJ contributed material and technical support for imaging. YHJ provided the Biotechnology Training support. KB and LW assisted with part of the manuscript review and editing process. YFX, ZLT, and XZX, as corresponding authors, provided guidance, supervision, and additional support in writing and editing the manuscript. All authors read and approved the final manuscript.

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### Data availability

No datasets were generated or analysed during the current study.

### Declarations

#### Ethics approval and consent to participate

This article contains experiments with animals that were approved by the Ethics Committee from South China Normal University (1129093).

#### Consent for publication

Not applicable.

#### Competing interests

The authors declare no competing interests.

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